



# Pulse Propagation in the Pulmonary Circulation

Nicholas A Hill<sup>1</sup>, Muhammad U Qureshi<sup>1,2</sup>

<sup>1</sup>School of Mathematics and Statistics, University of Glasgow, UK

<sup>2</sup>International Islamic University, Islamabad, Pakistan

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## Introduction

- Pulmonary circulation regulates an entire cardiac output under low pressure (10-25 mmHg) in normal conditions.
- Abnormally high pressure and significant shape changes in the pressure pulse under hypertensive conditions.
- Wave reflections, originating from junctions and microcirculation, contribute in shaping the pressure pulse.
- Seeking to understand the underlying mechanism of pulmonary pulse propagation under normal and abnormal conditions.
- Investigating the patterns of wave reflections and the parameters influencing their type and nature, such as the pulse wave velocity, due to vascular remodelling.

## The Model

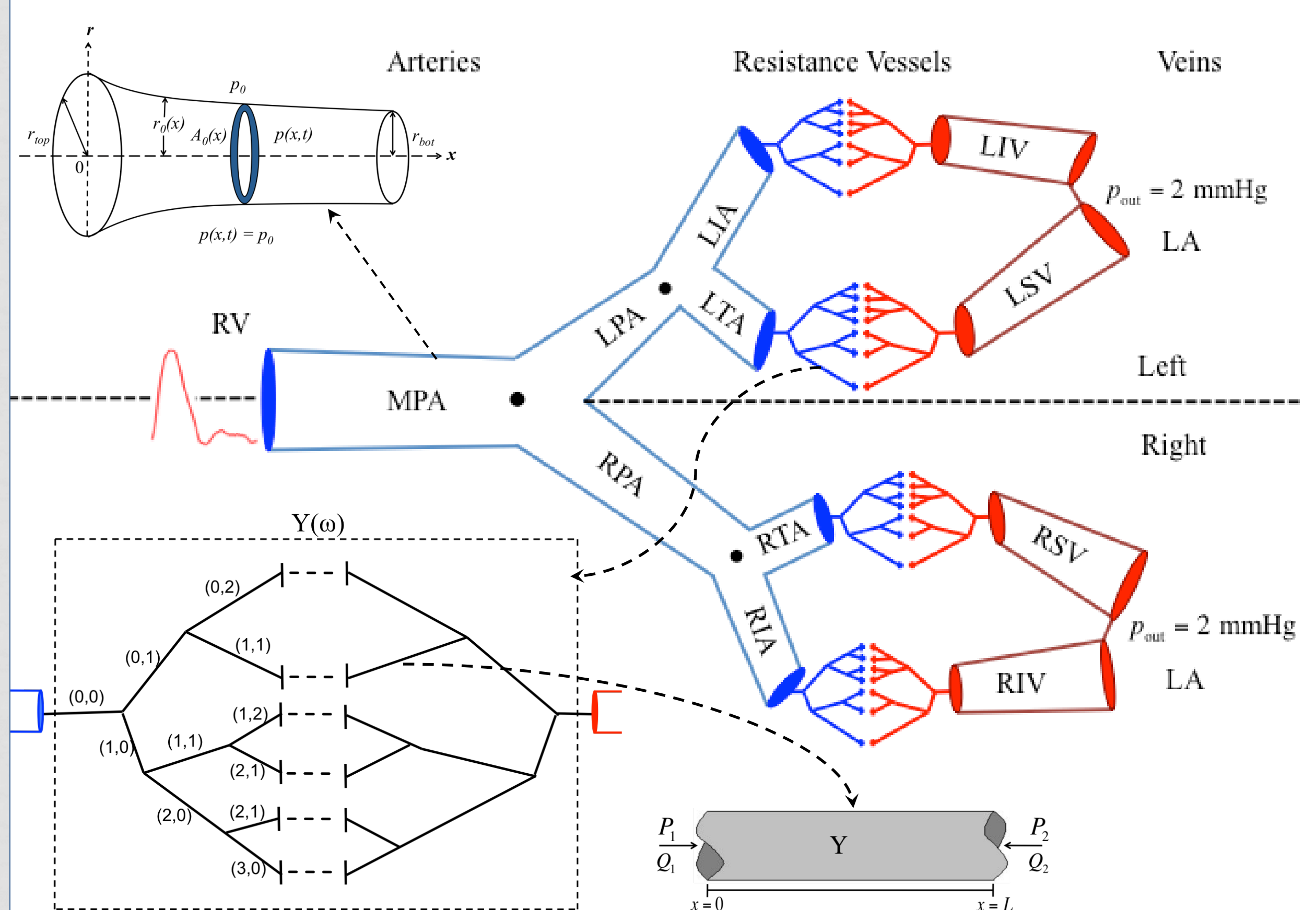


Figure 1. Schematics of basic components and their use in building a complete model of pulmonary system.

- A multi-scale mathematical and computational model.
- Includes both arterial and venous sides of the circulation.
- Patient-specific geometry using magnetic resonance imaging (MRI) for the first three generations of the large pulmonary arteries.
- 'Large arteries' connected with the corresponding 'large veins' via bifurcating and connected structured trees (vascular beds) of 'small vessels' with radii  $> 50 \mu\text{m}$ .
- Non-linear fluid dynamical model governing pressure and flow in the large vessels.
- Linearised flow equations for small vessels.

## Methods

- Conservation of Mass and Momentum

$$\frac{\partial q}{\partial x} + \frac{\partial A}{\partial t} = 0 \quad \frac{\partial q}{\partial t} + \frac{\partial}{\partial x} \left( \frac{q^2}{A} \right) + \frac{A}{\rho} \frac{\partial p}{\partial x} = -\frac{2\pi\nu R q}{\delta A}$$

- Equation of State

$$p(x,t) - p_0 = \frac{4 Eh}{3 r_0} \left( 1 - \sqrt{\frac{A_0}{A}} \right)$$

- Flow and Pressure In the Small Vessels In Frequency Space

$$Q(x, \omega) = a \cos(\omega x/c) + b \sin(\omega x/c)$$

$$P(x, \omega) = ig_{\omega}^{-1} (b \cos(\omega x/c) - a \sin(\omega x/c))$$

- Admittance Relation Connecting Large Arteries and Veins

$$\begin{pmatrix} Q_1 \\ Q_2 \end{pmatrix} = Y \begin{pmatrix} P_1 \\ P_2 \end{pmatrix}$$

## Examples of Results

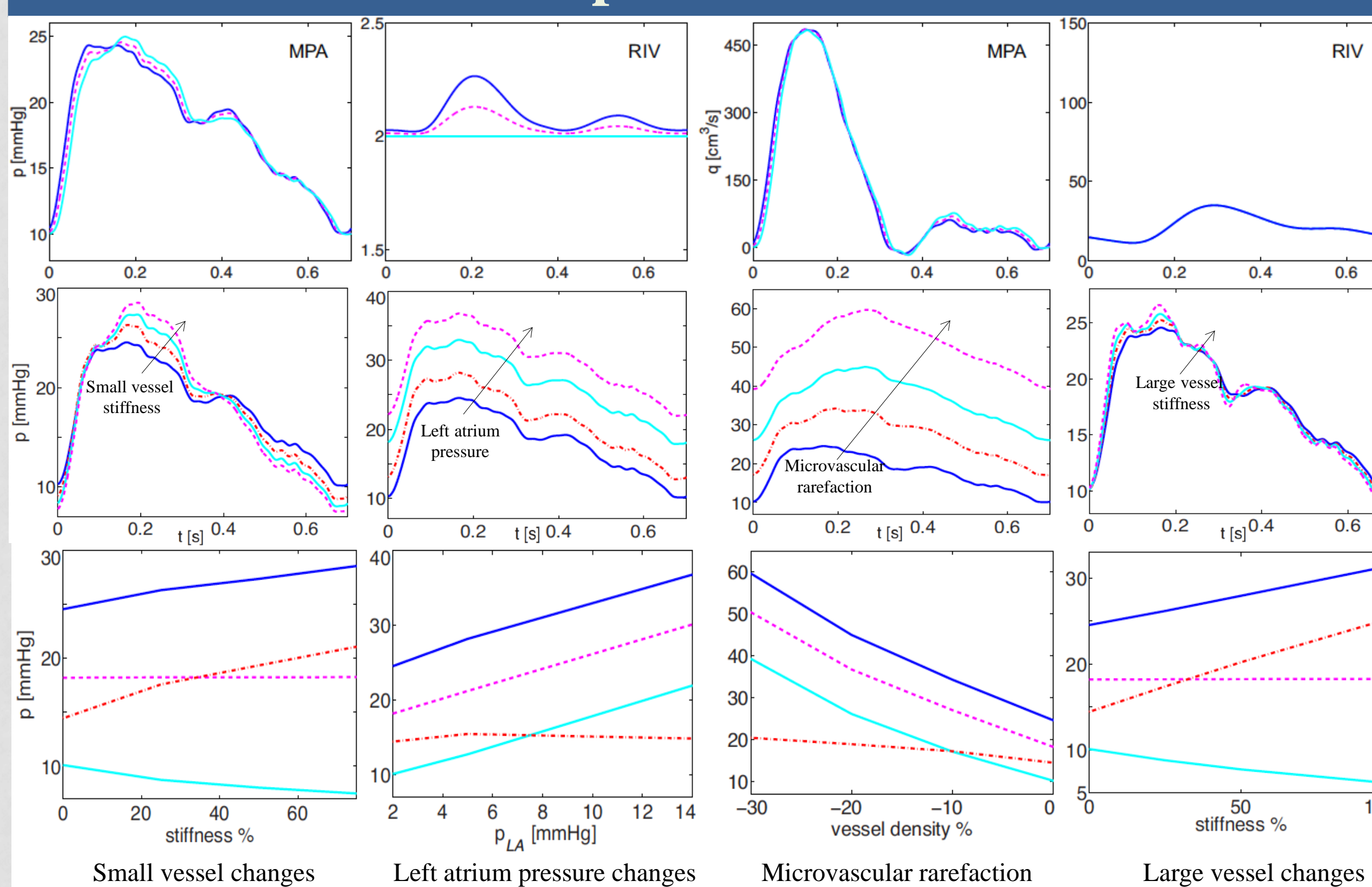


Figure 2. 1<sup>st</sup> Row: Pressure and flow profiles in the MPA and RIV, simulated at proximal, midpoint and distal locations. 2<sup>nd</sup> Row: Effects of pulmonary hypertension (PH) on pressure pulse in the MPA. 3<sup>rd</sup> Row: Effects of PH on mean (magenta), peak (blue), pulse (red) and trough (cyan) pressures in the MPA.

## Wave Intensity Analysis (WIA)

- Decomposition of pressure and velocity wavefronts into forward and backward components

$$dp_{\pm} = \frac{1}{2} (dp \pm \rho c(p) du), \quad du_{\pm} = \frac{1}{2} \left( du \pm \frac{dp}{\rho c(p)} \right)$$

- Wave Intensity

$$W_{\pm}^I = \frac{dp_{\pm}}{dt} \frac{du_{\pm}}{dt}$$

- Separated Pressure and Velocity

$$p_{\pm} = p_0 + \int_{t-T}^t dp_{\pm}, \quad u_{\pm} = u_0 + \int_{t-T}^t du_{\pm}$$

## Wave Reflections

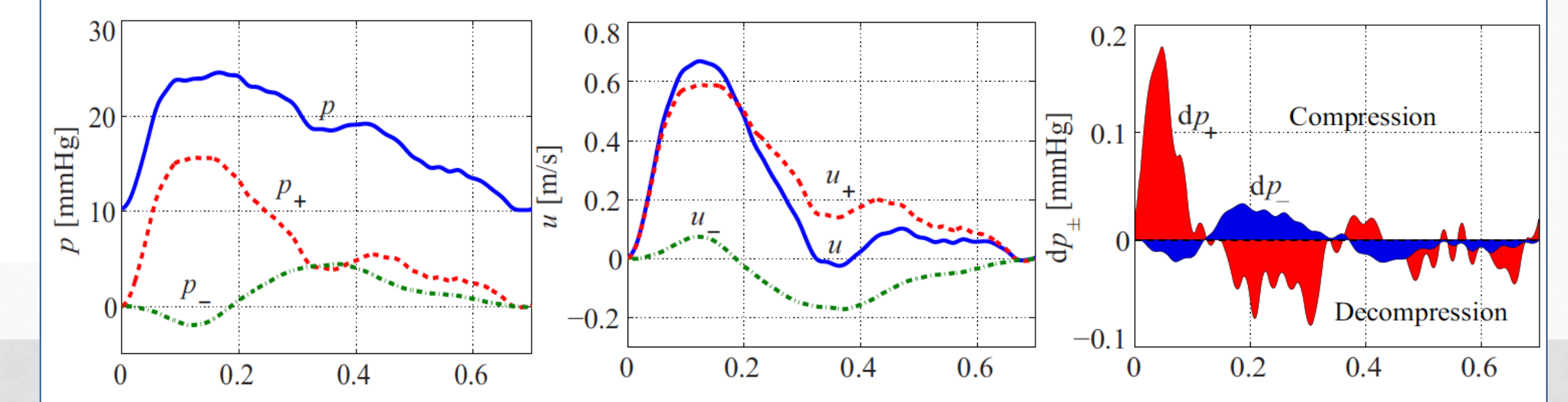


Figure 3. Separated profiles of pressure (left), velocity (center) and pressure wavefronts (right) at the midpoint location in the Main Pulmonary Artery.

- Forward Compression Wave

$$dp_{+} > 0$$

- Forward Decompression Wave

$$dp_{+} < 0$$

- Backward Compression Wave

$$dp_{-} > 0$$

- Backward Decompression Wave

$$dp_{-} < 0$$

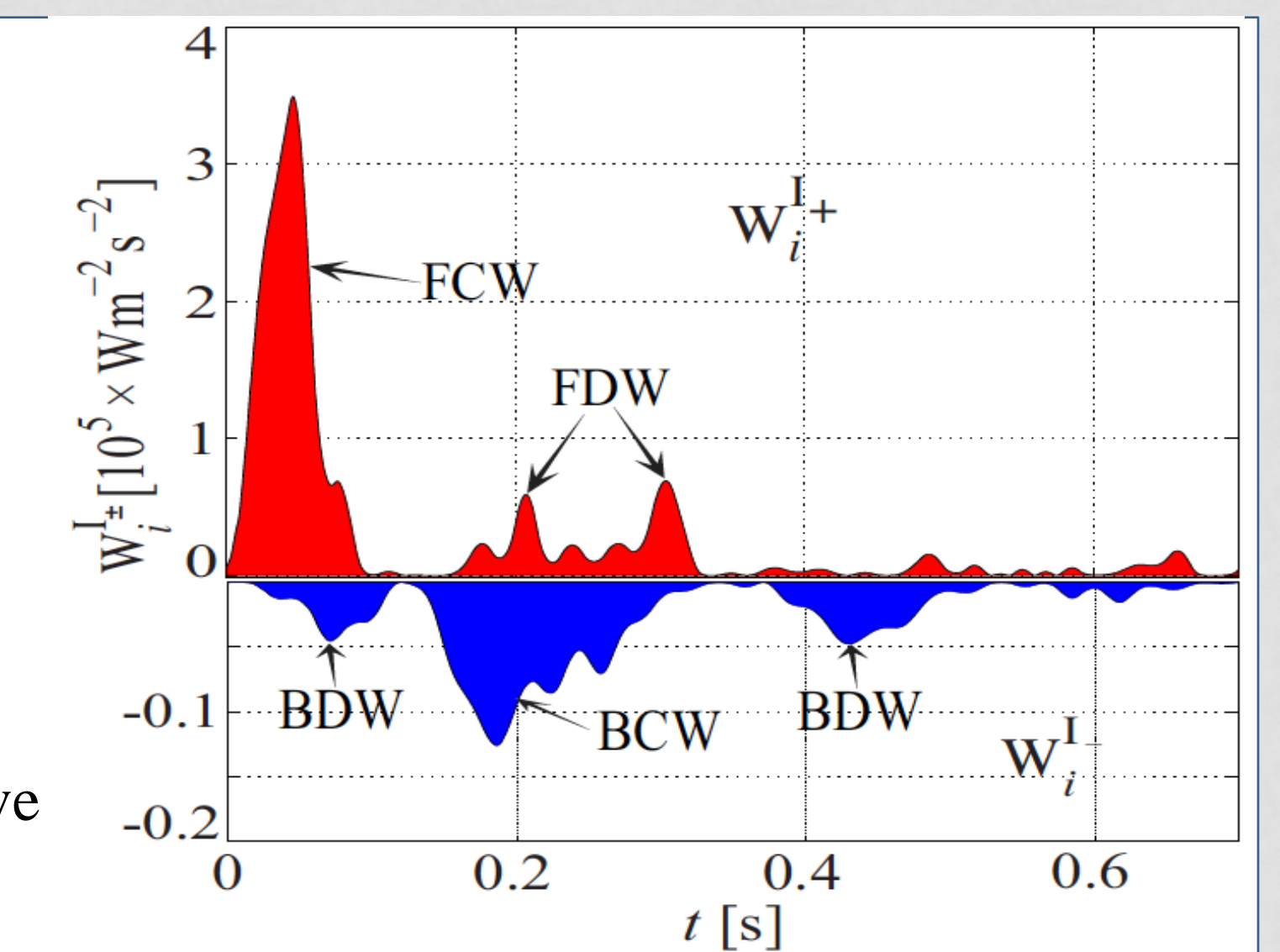


Figure 4. Separated wave intensity profiles in the MPA, identifying the types and direction of local waves.

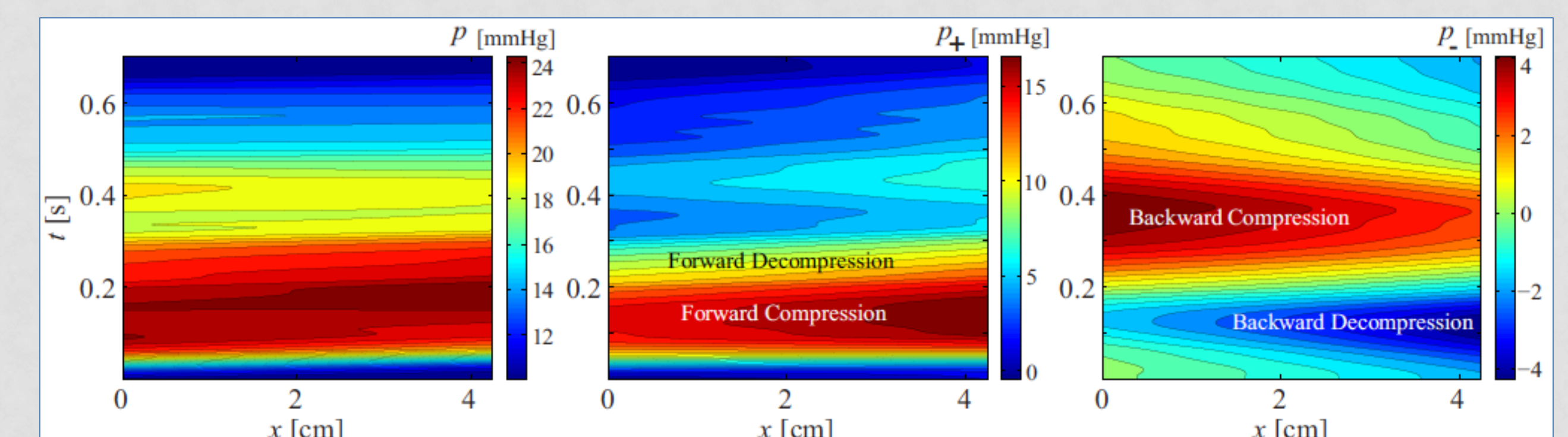


Figure 5. Contours of pressure waveform along the MPA in (x,t) space.

## Pulse Wave Velocity (PWV)

- P-U loop Method

$$c_{pu} = \frac{1}{\rho} \frac{dp}{du}$$

- Sum of Squares Technique

$$c_{ss} = \frac{1}{\rho} \sqrt{\frac{\sum dp^2}{\sum du^2}}$$

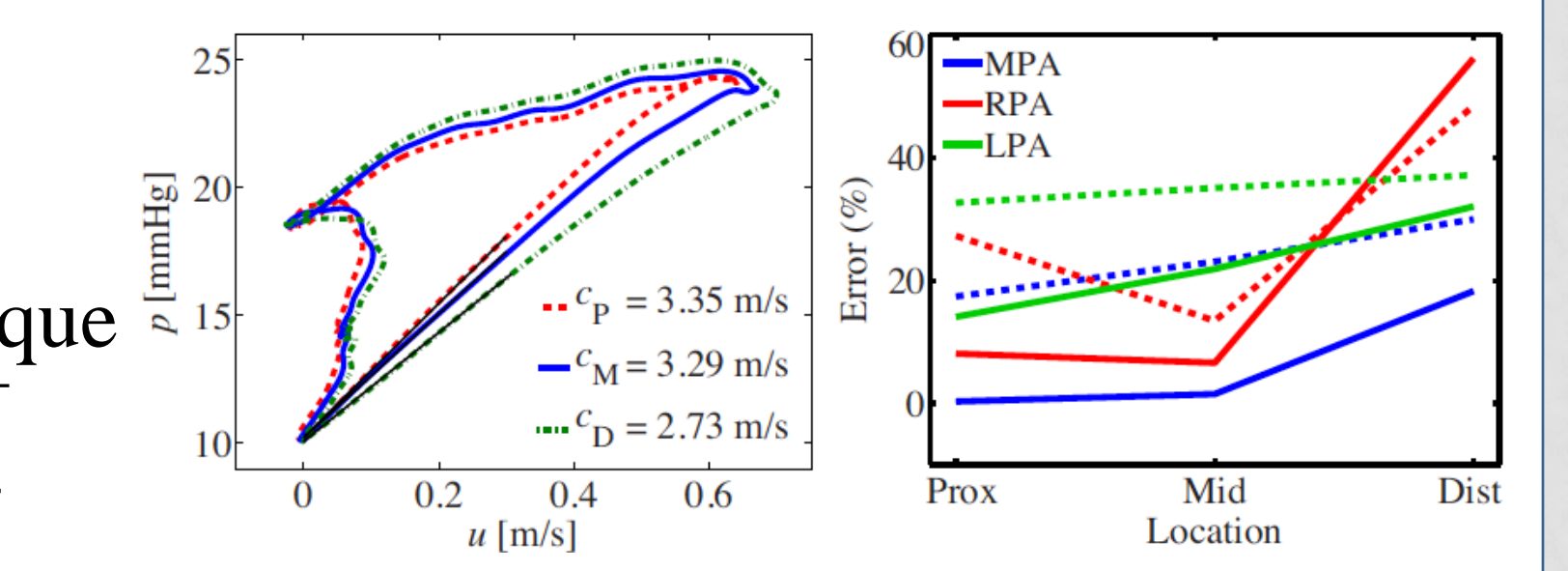


Figure 6. Left: P-U loops in the MPA. Right: Solid lines represent  $c_{pu}$  and dashed lines represent  $c_{ss}$ . The figure shows the error of PWV estimates about averaged theoretical PWV.

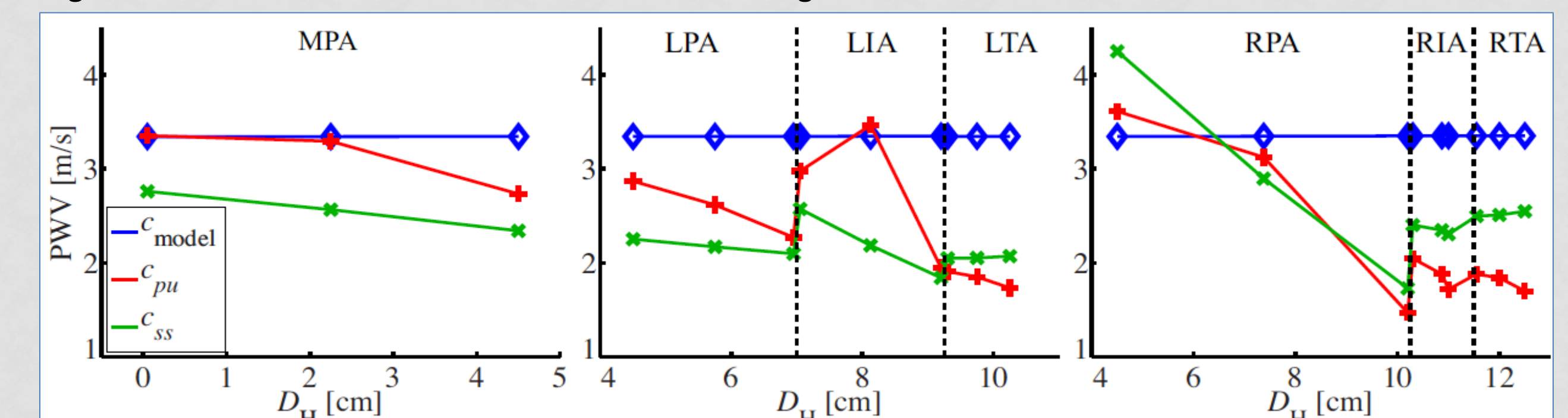


Figure 7. Left: P-U loops in the MPA. Right: Solid lines represent  $c_{pu}$  and dashed lines represent  $c_{ss}$ . The figure shows the error in PWV estimates about averaged theoretical PWV.

## Conclusions

- Increase in peak and pulse pressure during pulmonary hypertension
- WIA demonstrates early systolic negative and late systolic positive wave reflections in the MPA.
- P-U loop is better than Sum of Squares for estimating the PWV at proximal locations.

## Contact

Nicholas.Hill@glasgow.ac.uk

## References

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- Olufsen et al. (2012) Journal of Fluid Mechanics, 705:280 – 305
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