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INTRODUCTION

- Pulmonary hypertension (PH) is defined as a mean pulmonary arterial blood pressure ≥ 25 mmHg. Comorbid heart failure accounts for over 80% of incidents. PH has been recognized as the third most common cardiovascular condition behind coronary heart disease and systemic hypertension.
- Definitive diagnosis requires invasive right heart catheterization (RHC), typically performed 3-4 years after the disease onset. Despite advancements in drug therapy there is no cure.
- Disease progression is monitored via frequent noninvasive imaging and recurrent RHCs, increasing the risk of morbidity and infection.
- This study shows how non-invasive image acquisition combined with mathematical modeling, sensitivity analysis, and uncertainty quantification can be used to identify biomarkers modulated by disease.

MODEL

Conservation laws

- Conservation of mass

$$\frac{\partial A}{\partial t} + \frac{\partial q}{\partial x} = 0$$

- Conservation of momentum

$$\frac{\partial q}{\partial t} + \frac{\partial}{\partial x} \left(\frac{q^2}{A} \right) + \frac{A}{\rho} \frac{\partial p}{\partial x} = - \frac{2\pi r q}{\delta A}$$

- Constitutive equation

$$p(r_0, A) = \beta \left(\sqrt{\frac{A}{A_0}} - 1 \right), \quad \beta = \frac{4Eh}{3r_0}$$

Boundary conditions:

- Inflow:** Specified from measured flow data
- Junction conditions**

$$q_p = q_{d_1} + q_{d_2}, \quad p_p = p_{d_1} = p_{d_2}$$

- Outflow (Windkessel model)**

$$\frac{dp}{dt} - R_1 \frac{dq}{dt} = q \frac{R_1 + R_2}{R_2 C} - \frac{p}{R_2 C}$$

$$R_1 = r_1 R_{1,nom}, \quad R_T = R_1 + R_2 = r_T R_{T,nom}, \quad C_T = c C_{T,nom}$$

Parameters estimated minimizing the least squares cost

$$\hat{\theta} = \arg \min_{\theta} J(\theta), \quad \theta = \{r_1, r_T, c, \beta\}$$

$$J = \frac{1}{N} \sum_{i=1}^n (p(t_i, \theta) - p_{mpa}(t_i))^2$$

Pulmonary arterial network geometry variation

Vessel lengths, radius, and network connectivity obtained by segmenting micro-CT images from 7 healthy and 5 hypertensive (hypoxia induced) mice.

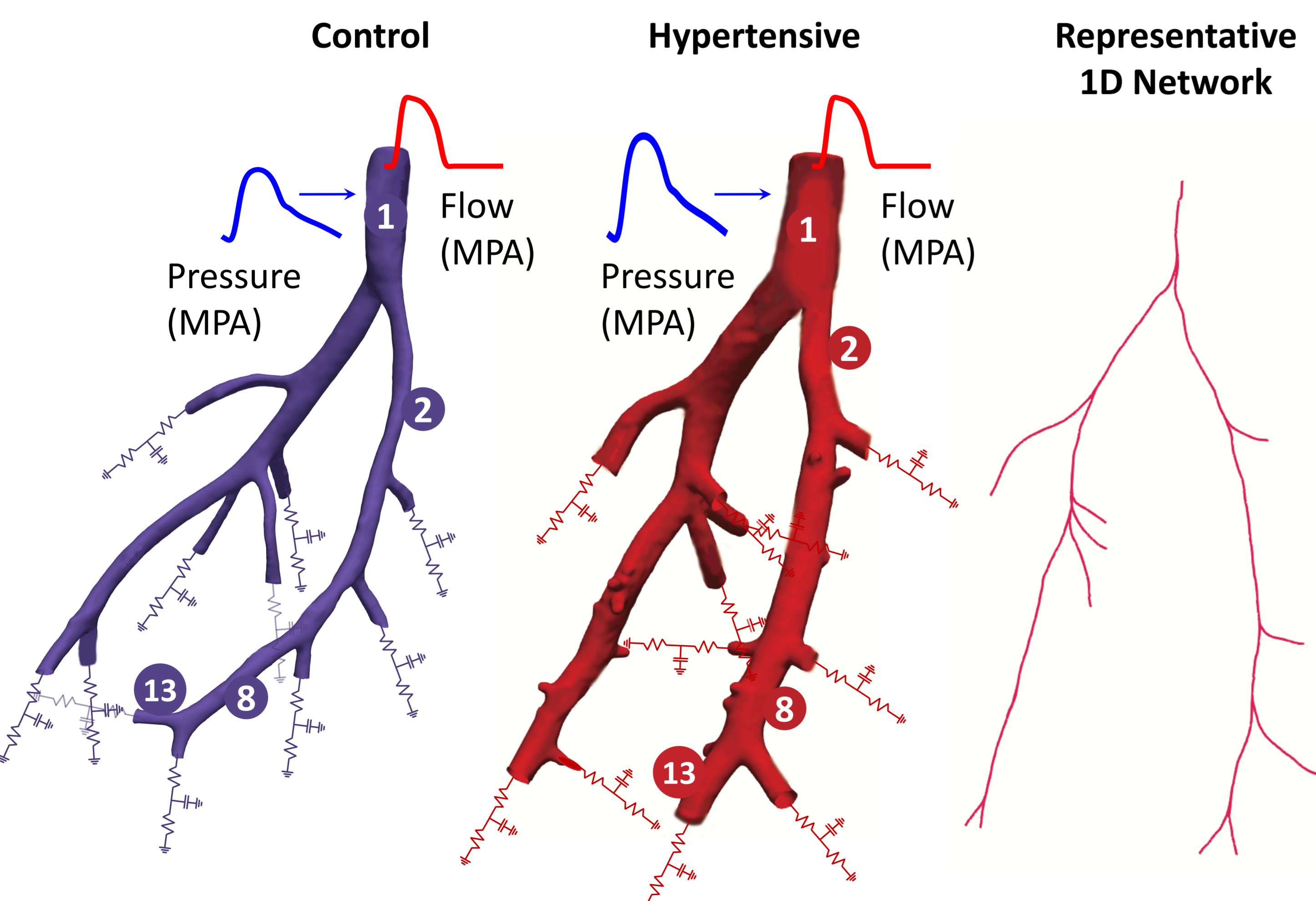


Fig 1. Representative control (blue) and hypertensive (red) networks extracted from micro-CT data.

SENSITIVITY ANALYSIS

- Local sensitivities

$$S(t, \theta_i) = \frac{\partial p_{mpa}(0, t, \theta)}{\partial \theta_i} \frac{\theta_i}{\bar{p}_{mpa}}, \quad \bar{S}(\theta_i) = \|S(t, \theta_i)\|_2$$

- Morris indices (global)

$$d^j(\theta_i) = \frac{f(\theta^j + e_i \Delta, t) - f(\theta^j, t)}{\Delta}, \quad j = 1, \dots, K, \quad \Delta = \frac{L}{2(L-1)}$$

$$\mu_i^* = \frac{1}{K} \sum_{j=1}^K |d_i^j|, \quad \sigma_i^2 = \frac{1}{K-1} \sum_{j=1}^K (d_i^j - \mu_i^*)^2$$

UNCERTAINTY QUANTIFICATION

- Confidence ($X = 0$) and prediction ($X = 1$) intervals (asymptotic)

$$y_l(t_i) = y(t_i, \hat{\theta}) \pm t_{n-p}^{\alpha/2} \hat{\sigma} (X + g_i (S^T S)^{-1} g_i)^{1/2}$$

where g_i^T is the i 'th row of the sensitivity matrix S , $\hat{\theta}$ are the optimized parameters, and $\hat{\sigma} = J$ is the estimated variance.

- DRAM: Credible intervals sampled from parameter distributions

$$\pi(\theta|y) = \frac{\pi(y|\theta)\pi_0(\theta)}{\pi(y)}$$

RESULTS

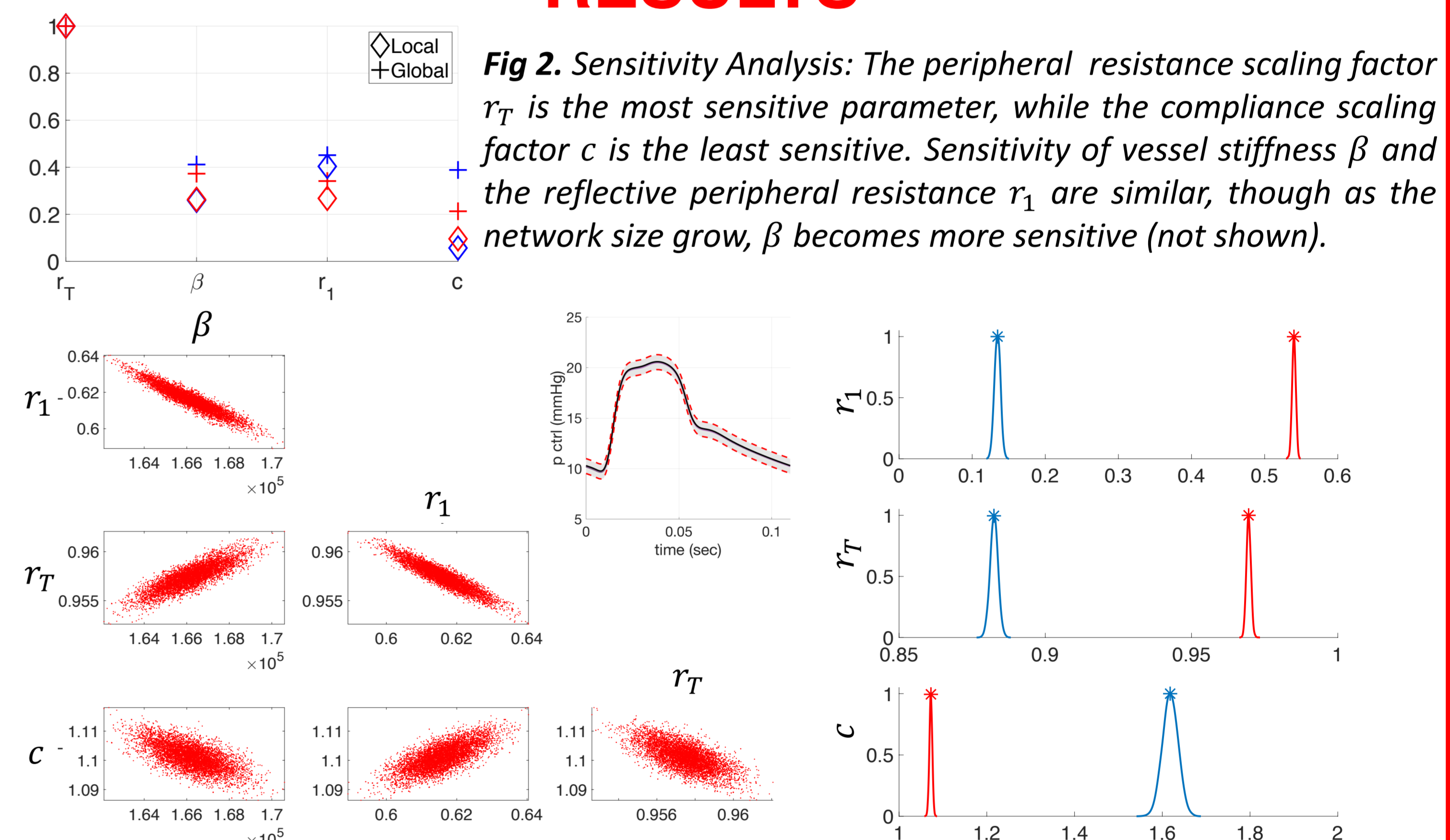


Fig 2. Sensitivity Analysis: The peripheral resistance scaling factor r_T is the most sensitive parameter, while the compliance scaling factor c is the least sensitive. Sensitivity of vessel stiffness β and the reflective peripheral resistance r_1 are similar, though as the network size grows, β becomes more sensitive (not shown).

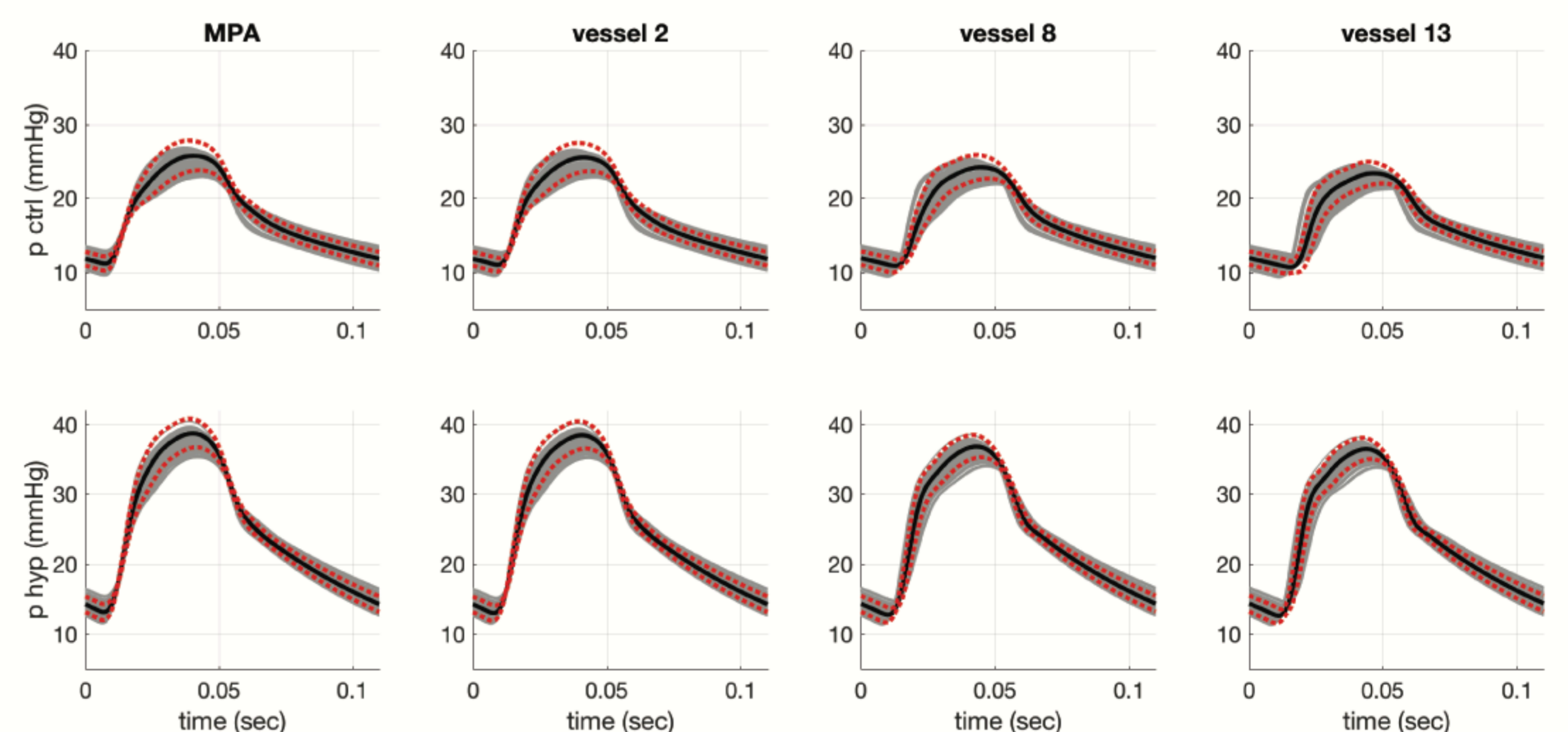


Fig 4. Predictions of pressure obtained from 1000 simulations varying the geometry (length and diameter) accounting for population variation (analysis on 7 control and 5 hypertensive mice). As expected geometry variation is more significant than variation around internal parameters (compare MPA panel with prediction intervals displayed above).

CONCLUSIONS

- The peripheral resistance scaling factor r_T is the most sensitive parameter.
- Parameters r_1 and β (and r_T) are correlated, fixing β gives an uncorrelated subset.
- Pressure predictions show that the variation with geometry is more influential than internal parameters $\theta = \{r_1, r_T, c, \beta\}$.
- Predictions of flow vary less (marked on Fig 1.) as it is specified at the inlet.